

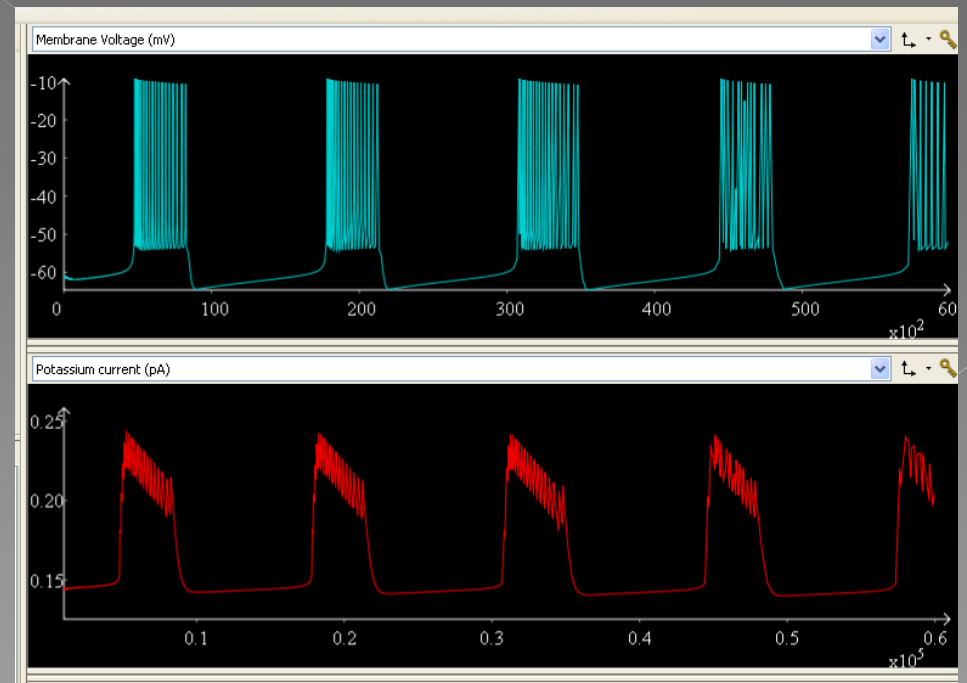
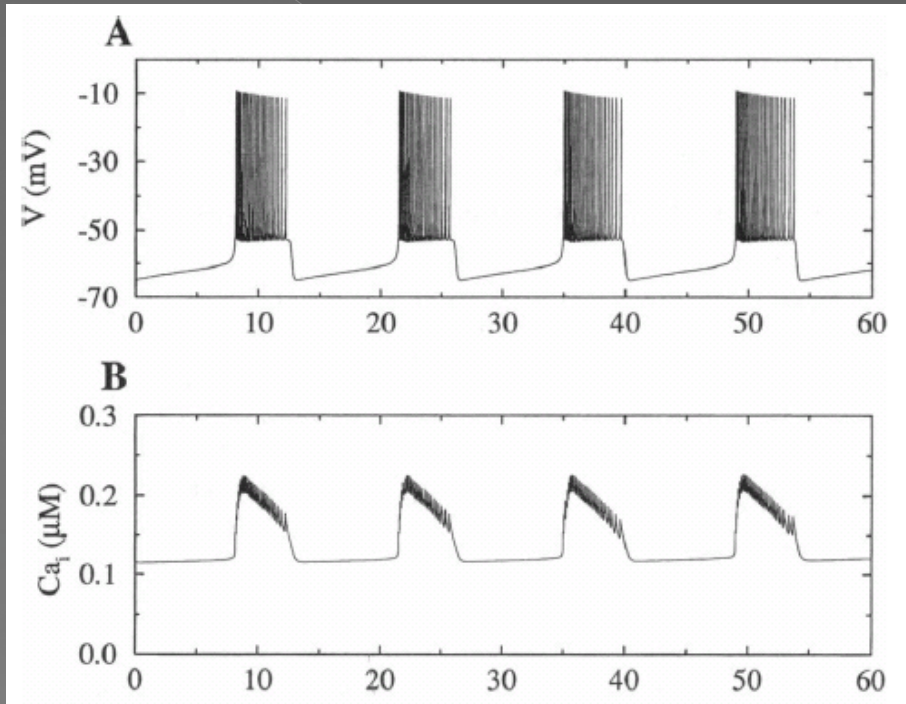
Model curation: the CellML approach

Catherine Lloyd
Auckland Bioengineering Institute



What is curation?

model validation



Publishing a model

model creation

```

current-----

[CfCa,RevPCa]= CalcConstantfield(Cai,Cao,2, Vm);
%Ca
[CfK,RevPK] = CalcConstantfield(Ki,Ko,1, Vm); %K
[CfNa,RevPNa] = CalcConstantfield(Nai,Nao,1,
Vm); %Na
if (count ==1 && currenttime == 0)
    Va = -74.0078;
else
    Va = Vm;
end
if (count ==0)
    [mcal, hcal,n] = calcRateConst(1,Va,
0,Cai,mcal,hcal,count,dt); %Calc m and h
    ICalNa = (0.00005*PCAL*CfNa)*mcal*hcal;
    ICalK = (0.001 * PCAL * CfK)*mcal*hcal;
    %ICaLNa = (PCAL * CfCa*mcal*hcal); %original
    ICalCa = (PCAL * CfCa*mcal*hcal);
    ICal = ICalCa + ICalK+ICaLNa;
else
    ICalNa = (0.00005*PCAL*CfNa)*mcal*hcal;
    ICalK = (0.001 * PCAL * CfK)*mcal*hcal;
    ICalCa = (PCAL * CfCa*mcal*hcal);
    ICal = ICalCa + ICalK+ICaLNa;
    [mcal, hcal] = calcRateConst(1,Va,
0,Cai,mcal,hcal,count,dt); %Calc m and h
end
    
```

Publishing a model

model creation



translated into text and equations for publication

which cotransporters are to be included in the model. Note that eqs. (3) imply that the total number of Cl^- and HCO_3^- ions and the sum of the number of K^+ and Na^+ ions in the ECS and the astrocyte are conserved at any time. Ion flux through KCCl , NKCCl ^[52] and NBC ^[45, 53] is modeled in a Nernst-like fashion, i.e.

$$(5) \quad J_{\text{KCCl}} = \frac{g_{\text{KCCl}}}{F} \frac{RT}{F} \ln \left(\frac{[\text{K}^+]_o [\text{Cl}^-]_o}{[\text{K}^+]_i [\text{Cl}^-]_i} \right),$$

$$(6) \quad J_{\text{NBC}} = \frac{g_{\text{NBC}}}{F} [V_m - E_{\text{NBC}}],$$

$$(7) \quad J_{\text{NKCCl}} = \frac{g_{\text{NKCCl}}}{F} \frac{RT}{F} \ln \left(\frac{[\text{Na}^+]_o [\text{K}^+]_o ([\text{Cl}^-]_o)^2}{[\text{Na}^+]_i [\text{K}^+]_i ([\text{Cl}^-]_i)^2} \right).$$

Here, g_{NKCCl} , g_{KCCl} and g_{NBC} are the conductances per unit area for the NKCCl , the KCCl and NBC cotransporter, respectively. The reversal potential of NBC is

$$(8) \quad E_{\text{NBC}} = \frac{RT}{z_{\text{NBC}} F} \ln \left(\frac{[\text{Na}^+]_o [\text{HCO}_3^-]_o}{[\text{Na}^+]_i [\text{HCO}_3^-]_i} \right),$$

where z_{NBC} is the effective valence of the NBC cotransporter complex, here taken to be -1, setting $z_{\text{NBC}} = -(n - 1) = -1$ where n is the stoichiometry, and adopting $n = 2$.

The assumed electroneutrality condition demands that the algebraic sum of all electric currents into the astrocyte has to be zero at every instant. The astrocytic membrane potential V_m is then given by solving the resulting equation with respect to V_m :

$$(9) \quad V_m = \frac{g_{\text{Na}} E_{\text{Na}} + g_{\text{K}} E_{\text{K}} + g_{\text{Cl}} E_{\text{Cl}} + \theta_{\text{NBC}} g_{\text{NBC}} E_{\text{NBC}} - J_{\text{NaKATPase}} F}{g_{\text{Na}} + g_{\text{K}} + g_{\text{Cl}} + \theta_{\text{NBC}} g_{\text{NBC}}}.$$

The rate of change of the astrocytic volume relative to its surface area, $w_a = v_i/A$, is, by

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The cell membrane is modeled as a capacitor connected in parallel with variable resistances and batteries representing the different ionic currents and pumps. The electrophysiological behavior of a single cell can hence be described with the following differential equation (23)

$$\frac{dV}{dt} = -\frac{I_{ion} + I_{stim}}{C_m} \quad (1)$$

where V is voltage, t is time, I_{ion} is the sum of all transmembrane ionic currents, I_{stim} is the externally applied stimulus current, and C_m is cell capacitance per unit surface area.

Similarly, ignoring the discrete character of microscopic cardiac cell structure, a 2D sheet of cardiac cells can be modeled as a continuous system with the following partial differential equation (23)

$$\frac{\partial V}{\partial t} = -\frac{I_{ion} + I_{stim}}{C_m} + \frac{1}{\rho_x S_x C_m} \frac{\partial^2 V}{\partial x^2} + \frac{1}{\rho_y S_y C_m} \frac{\partial^2 V}{\partial y^2} \quad (2)$$

where ρ_x and ρ_y are the cellular resistivity in the x and y directions, S_x and S_y are the surface-to-volume ratio in the x and y directions, and I_{ion} is the sum of all transmembrane ionic currents given by the following equation

$$I_{ion} = I_{Na} + I_{K1} + I_{to} + I_{Kr} + I_{Ks} + I_{CaL} + I_{NaCa} + I_{NaK} + I_{pCa} + I_{pK} + I_{bCa} + I_{bK} \quad (3)$$

where I_{NaCa} is $\text{Na}^+/\text{Ca}^{2+}$ exchanger current, I_{NaK} is Na^+/K^+ pump current, I_{pCa} and I_{pK} are plateau Ca^{2+} and K^+ currents, and I_{bCa} and I_{bK} are background Ca^{2+} and K^+ currents.

model creation



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```
%-----Calc the L-type Ca
current-----

[CfCa,RevPCa]= CalcConstantfield(Cai,Cao,2,
Vm); %Ca
[CfK,RevPK] = CalcConstantfield(Ki,Ko,1, Vm);
%K
[CfNa,RevPNa] = CalcConstantfield(Nai,Nao,
1, Vm); %Na
if (count ==1 && currenttime == 0)
    Va = -74.0078;
else
    Va = Vm;
end
if (count ==0)
    [mcal, hcal,n] = calcRateConst(1,Va,
0,Cai,mcal,hcal,count,dt); %Calc m and h
    ICalNa = (0.00005*PCAL*CfNa)*mcal*hcal;
    ICalK = (0.001 * PCAL * CfK)*mcal*hcal;
    %ICaLca = (PCAL * CfCa*mcal*hcal);
%original
    ICalCa = (PCAL * CfCa*mcal*hcal);
    ICal = ICalCa + ICalK+ICalNa;
else
    ICalNa = (0.00005*PCAL*CfNa)*mcal*hcal;
    ICalK = (0.001 * PCAL * CfK)*mcal*hcal;
    ICalCa = (PCAL * CfCa*mcal*hcal);
    ICal = ICalCa + ICalK+ICalNa;
    [mcal, hcal] = calcRateConst(1,Va,
0,Cai,mcal,hcal,count,dt); %Calc m and h
end
```

model creation



translated into text and
equations for publication



reviewed & published



interpreted & implemented

Publishing a model

```
%-----Calc the L-type Ca
current-----

[CfCa,RevPCa]= CalcConstantfield(Cai,Cao,2,
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%K
[CfNa,RevPNa] = CalcConstantfield(Nai,Nao,
1, Vm); %Na
if (count ==1 && currenttime == 0)
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    Va = Vm;
end
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0,Cai,mcal,hcal,count,dt); %Calc m and h
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    ICalK = (0.001 * PCAL * CfK)*mcal*hcal;
    %ICaLca = (PCAL * CfCa*mcal*hcal);
%original
    ICalCa = (PCAL * CfCa*mcal*hcal);
    ICal = ICalCa + ICalK+ICalNa;
else
    ICalNa = (0.00005*PCAL*CfNa)*mcal*hcal;
    ICalK = (0.001 * PCAL * CfK)*mcal*hcal;
    ICalCa = (PCAL * CfCa*mcal*hcal);
    ICal = ICalCa + ICalK+ICalNa;
    [mcal, hcal] = calcRateConst(1,Va,
0,Cai,mcal,hcal,count,dt); %Calc m and h
end
```

model creation



error

translated into text and
equations for publication



error

reviewed & published



error

interpreted & implemented

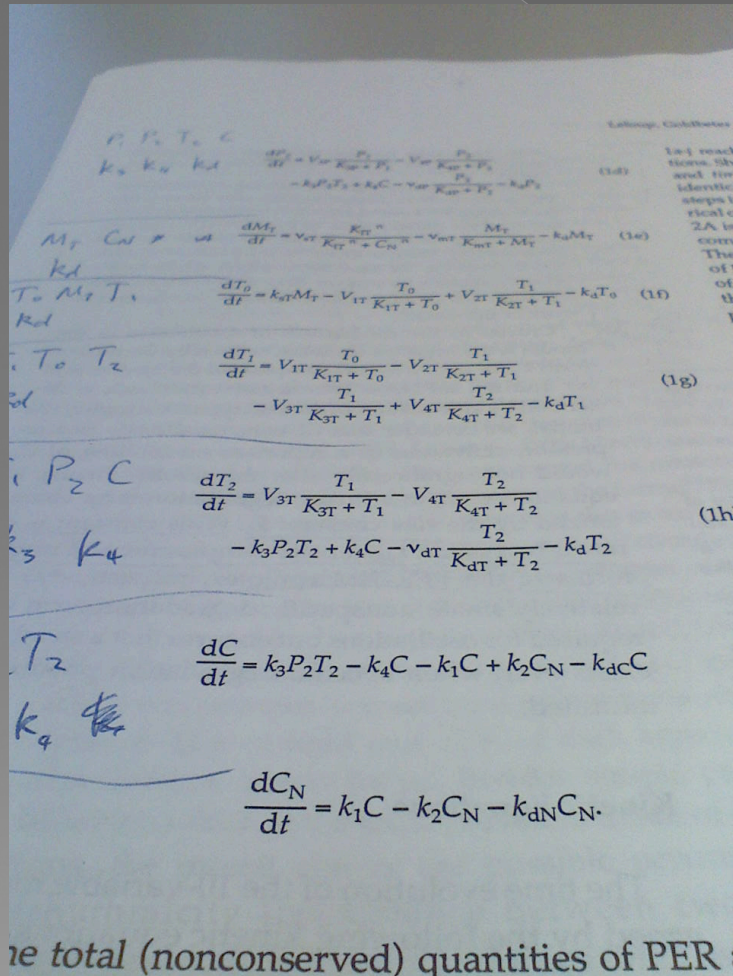
The reality...

- ◉ There are >450 models in the repository
- ◉ Only a handful been translated straight from the published paper into a working CellML model
- ◉ Typographical errors
- ◉ Missing parameter values
- ◉ Missing initial conditions
- ◉ Missing equations
- ◉ Lack of unit definitions

Step 1: model translation

Published paper

CellML



Handwritten mathematical equations from a published paper, showing differential equations for variables M_T , T_0 , T_1 , T_2 , C , and C_N . The equations are labeled (1d), (1e), (1f), (1g), (1h), and (1i).

$$\frac{dM_T}{dt} = V_{IT} \frac{K_{IT}^n}{K_{IT}^n + C_N} - V_{OT} \frac{M_T}{K_{OT} + M_T} - k_d M_T \quad (1d)$$

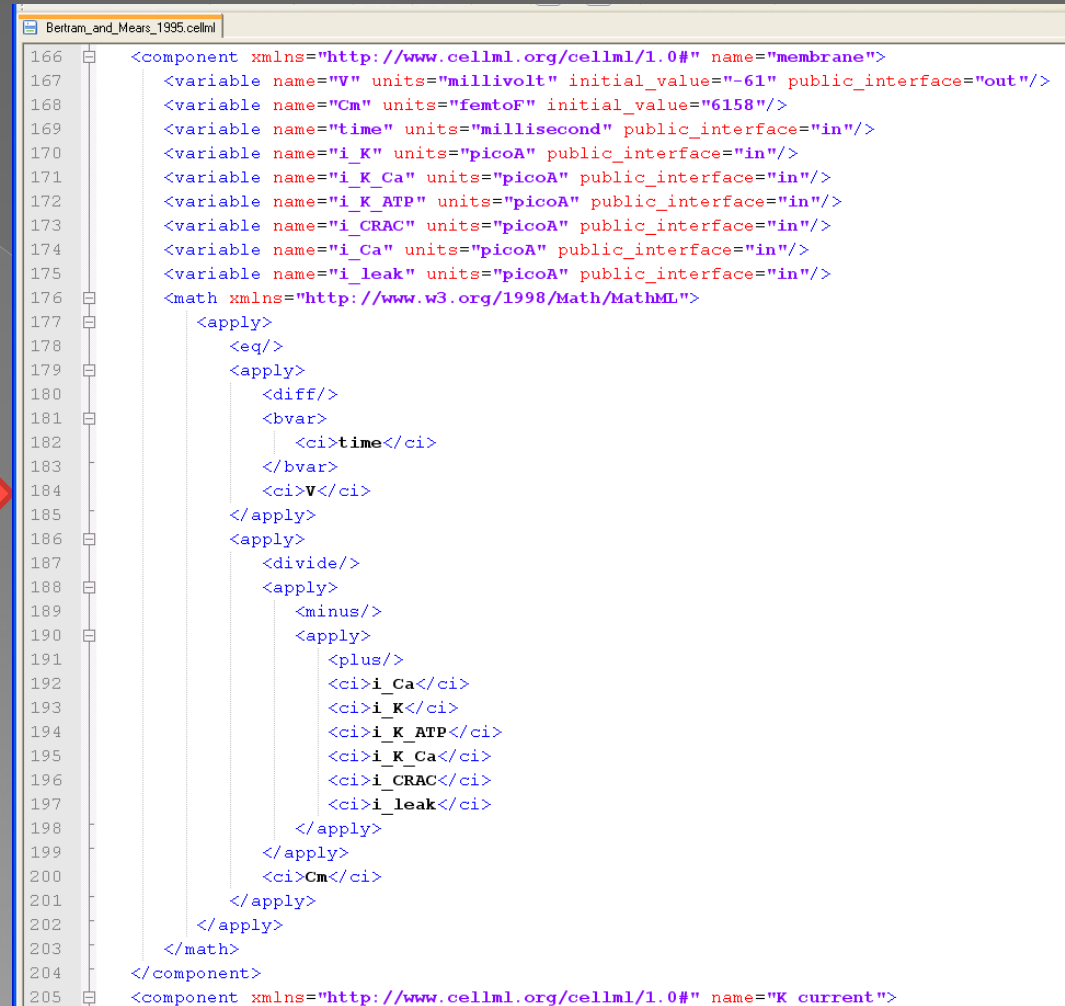
$$\frac{dT_0}{dt} = k_{dT} M_T - V_{IT} \frac{T_0}{K_{IT} + T_0} + V_{2T} \frac{T_1}{K_{2T} + T_1} - k_d T_0 \quad (1e)$$

$$\frac{dT_1}{dt} = V_{IT} \frac{T_0}{K_{IT} + T_0} - V_{2T} \frac{T_1}{K_{2T} + T_1} - V_{3T} \frac{T_1}{K_{3T} + T_1} + V_{4T} \frac{T_2}{K_{4T} + T_2} - k_d T_1 \quad (1f)$$

$$\frac{dT_2}{dt} = V_{3T} \frac{T_1}{K_{3T} + T_1} - V_{4T} \frac{T_2}{K_{4T} + T_2} - k_3 P_2 T_2 + k_4 C - v_{dT} \frac{T_2}{K_{dT} + T_2} - k_d T_2 \quad (1g)$$

$$\frac{dC}{dt} = k_3 P_2 T_2 - k_4 C - k_1 C + k_2 C_N - k_{dC} C \quad (1h)$$

$$\frac{dC_N}{dt} = k_1 C - k_2 C_N - k_{dN} C_N \quad (1i)$$



Screenshot of a CellML model translation from a published paper to a CellML file. The model is named "membrane" and contains several variables and equations.

```

166 <component xmlns="http://www.cellml.org/cellml/1.0#" name="membrane">
167   <variable name="V" units="millivolt" initial_value="-61" public_interface="out"/>
168   <variable name="Cm" units="femtoF" initial_value="6158"/>
169   <variable name="time" units="millisecond" public_interface="in"/>
170   <variable name="i_K" units="picoA" public_interface="in"/>
171   <variable name="i_K_Ca" units="picoA" public_interface="in"/>
172   <variable name="i_K_ATP" units="picoA" public_interface="in"/>
173   <variable name="i_CRAC" units="picoA" public_interface="in"/>
174   <variable name="i_Ca" units="picoA" public_interface="in"/>
175   <variable name="i_leak" units="picoA" public_interface="in"/>
176   <math xmlns="http://www.w3.org/1998/Math/MathML">
177     <apply>
178       <eq/>
179       <apply>
180         <diff/>
181         <bvar>
182           <ci>time</ci>
183         </bvar>
184         <ci>V</ci>
185       </apply>
186       <apply>
187         <divide/>
188         <apply>
189           <minus/>
190           <apply>
191             <plus/>
192             <ci>i_K</ci>
193             <ci>i_K_Ca</ci>
194             <ci>i_K_ATP</ci>
195             <ci>i_CRAC</ci>
196             <ci>i_leak</ci>
197           </plus/>
198           <ci>Cm</ci>
199         </apply>
200       </divide/>
201     </math>
202   </component>
203   <component xmlns="http://www.cellml.org/cellml/1.0#" name="K current">

```

[illegible]

Step 3: simulation comparisons

9110 Cell Biology: Goldbeter

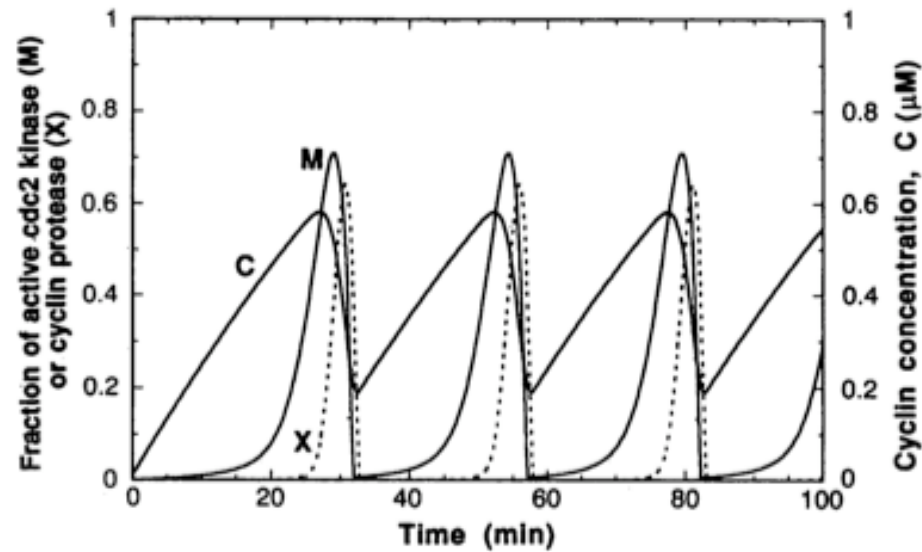
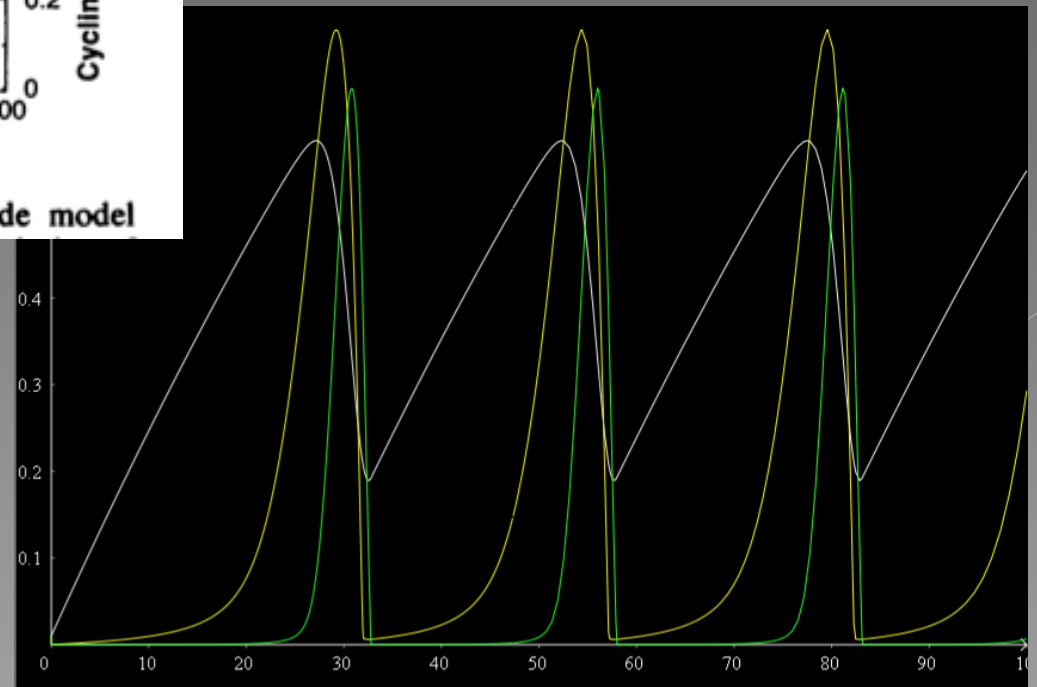


FIG. 3. Sustained oscillations in the minimal cascade model



```

582 </apply>
583 </apply>
584 </math>
585 </component>
586 <component name="L_type_Ca_channel">
587   <variable units="picoA" public_interface="out" name="i_Ca_L"/>
588   <variable units="nanoS" name="g_Ca_L" initial_value="6.75"/>
589   <variable units="millivolt" name="E_Ca_app" initial_value="60"/>
590   <variable units="dimensionless" name="f_Ca"/>
591   <variable units="millimolar" name="k_Ca" initial_value="0.025"/>
592   <variable units="second" public_interface="in" private_interface="out" name="time"/>
593   <variable units="millivolt" public_interface="in" private_interface="out" name="V"/>
594   <variable units="millimolar" public_interface="in" name="Ca_d"/>
595   <variable units="dimensionless" private_interface="in" name="d_L"/>
596   <variable units="dimensionless" private_interface="in" name="f_L_1"/>
597   <variable units="dimensionless" private_interface="in" name="f_L_2"/>
598   <math xmlns="http://www.w3.org/1998/Math/MathML">
599     <apply>
600       <eq/>
601       <ci>i_Ca_L</ci>
602       <apply>
603         <times/>
604         <ci>g_Ca_L</ci>
605         <ci>d_L</ci>
606         <apply>
607           <plus/>
608           <apply>
609             <times/>
610             <ci>f_Ca</ci>
611             <ci>f_L_1</ci>
612           </apply>
613           <apply>
614             <times/>
615             <apply>
616               <minus/>
617               <cn cellml:units="dimensionless">1</cn>
618               <ci>f_Ca</ci>
619             </apply>
620             <ci>f_L_2</ci>
621           </apply>

```

The current situation

- After a long period without tools we now have a legacy of broken models to curate
- Of the 450 models in the repository $\sim 1/2$ have been curated to some degree
- We accept there are some models which will never work properly

Future work

- ◉ Continuing to validate the models in the repository (existing and new)
- ◉ Model annotation
- ◉ Automated curation?
- ◉ Replace the curation star system with a more meaningful set of curation “flags”



Acknowledgements

