

# Methods for Semantic Cell Modelling and Convenient Simulation

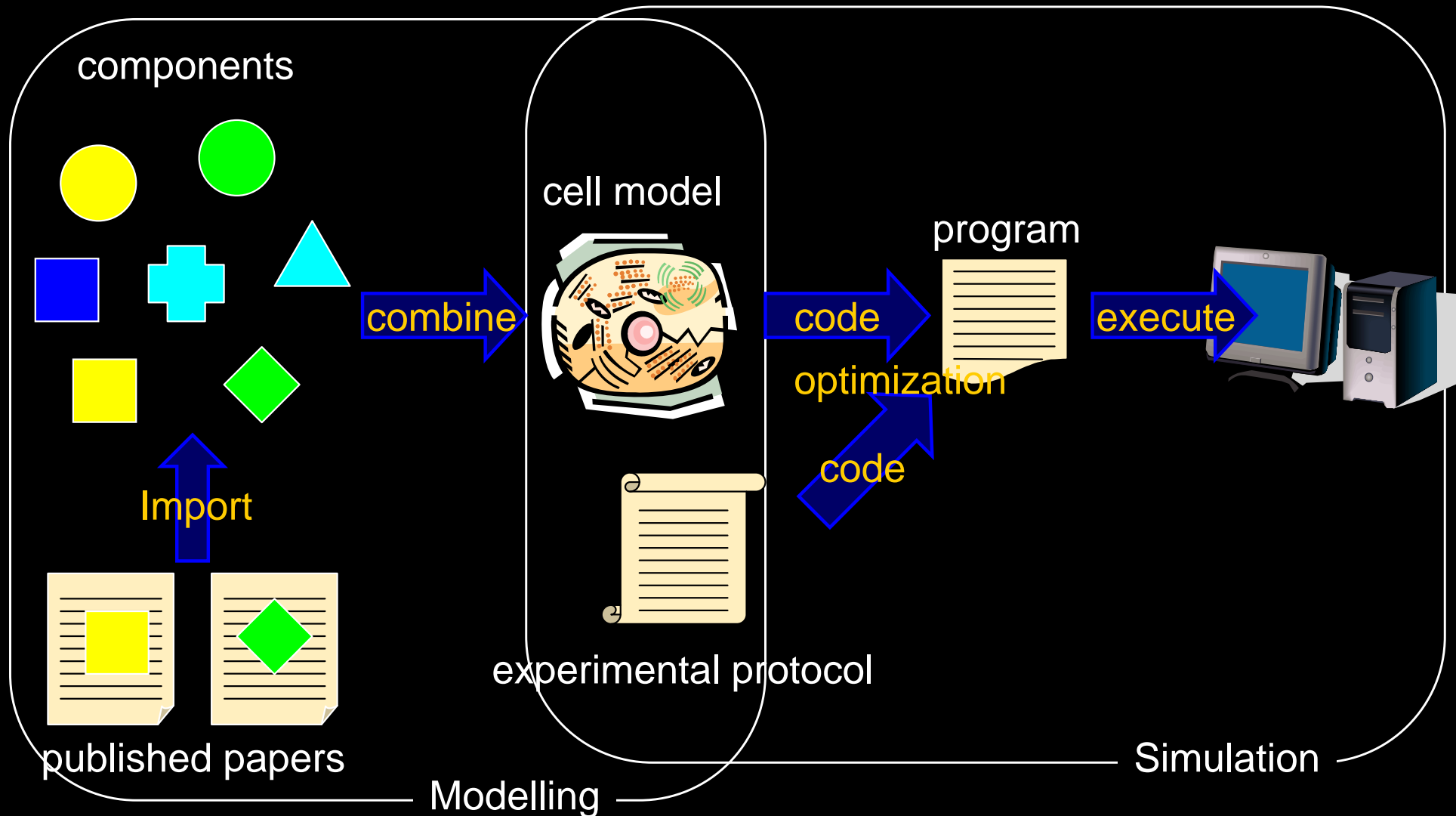
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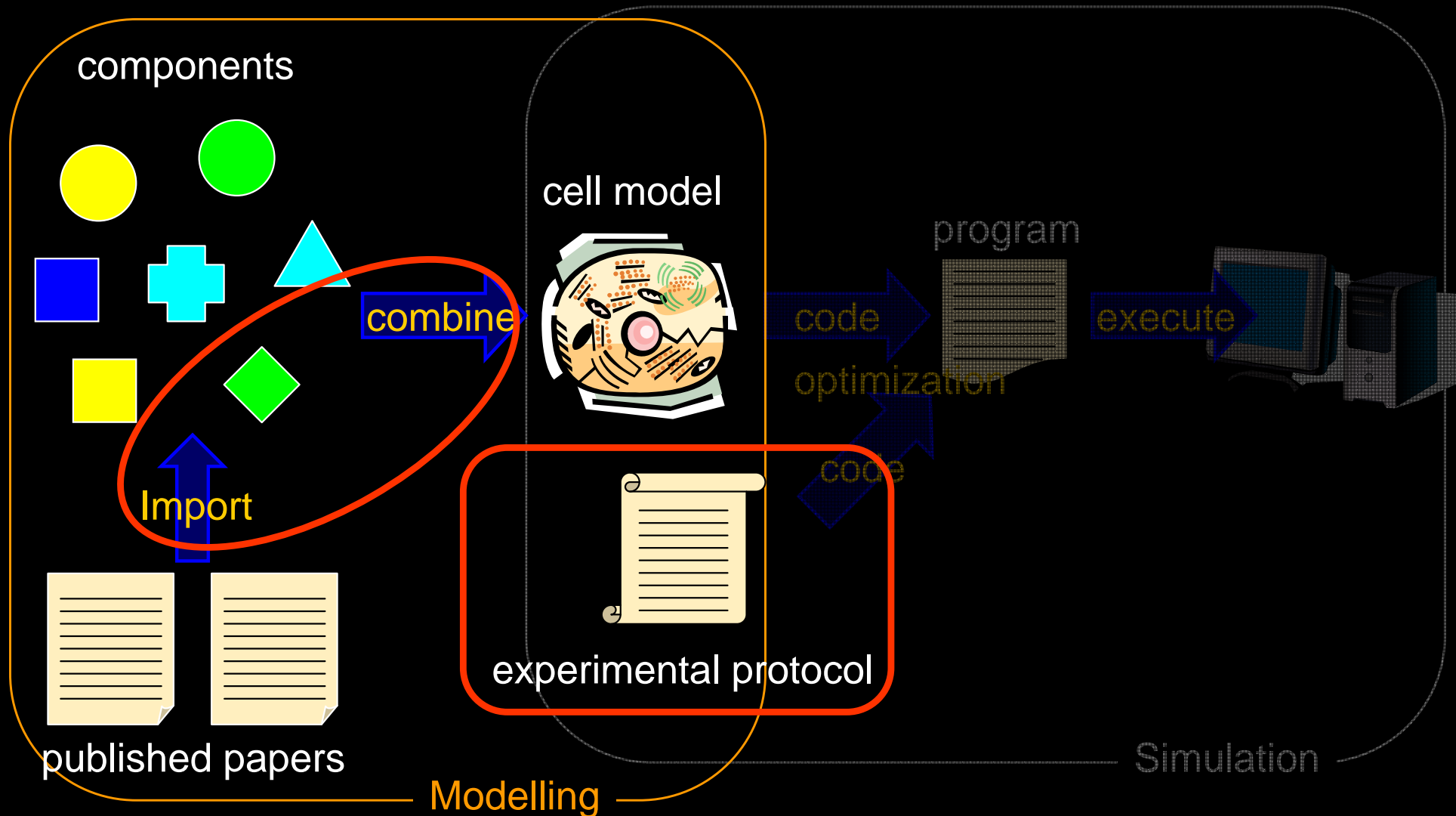
# Current Status of Kyoto Model

- Kyoto Model:
  - Comprehensive cardiac myocyte model
  - Recent model published
    - Kuzumoto, et. al. *Prog Biophys Mol Biol*. 2008.  
doi: 10.1016/j.pbiomolbio.2007.07.005
  - CellML files
    - Being written for several variants of Kyoto Model

# Modelling & Simulation

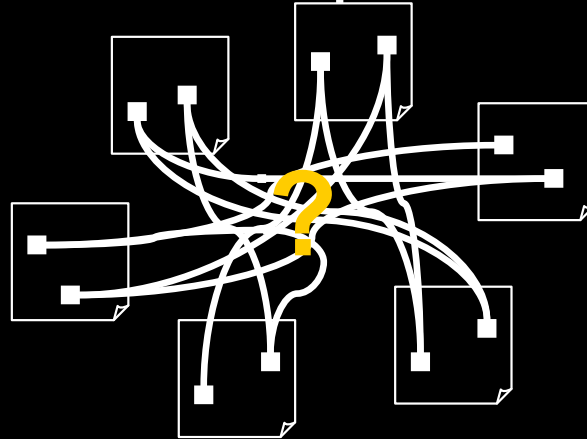


# Methods for Modelling



# Computer Aided Modelling

- Troublesome task in editing models
  - Composition of components



- Modelling with Ontology
  - Semantic annotation to model components
  - Intelligent assistance using Ontology

# Edit of Component

The screenshot shows the 'Model Component Editor' window. At the top, there are 'File' and 'Edit' menus. Below that, the 'Component name' is 'ICaL' and the 'ID' is '543'. The 'Description' is 'L-type calcium channel'. A table of 'Variables' is shown below, with columns for name, math, unit, id, local, default, and desc. The variables listed are ICaL, Vshift, and Vshift0. Below the variables table is the 'Equations' section, which displays three mathematical equations for  $k_{APRP}$ ,  $k_{RIAI}$ , and  $k_{AIRI}$ . The equation for  $k_{RIAI}$  is highlighted in blue. At the bottom, there is a text input field for the equation and a description field.

Component name: ICaL ID: 543  
Description: L-type calcium channel

name	math	unit	id	local	default	desc
ICaL	$I_{CaL}$	pA/pF	245	<input type="checkbox"/>		
Vshift	$V_{shift}$	mV		<input checked="" type="checkbox"/>		
Vshift0	$V_{shift0}$	mV				

Equations

$$k_{APRP} = \frac{1}{480.0 \cdot e^{\frac{V_m + V_{shift}}{7.0}} + 2.2 \cdot e^{\frac{V_m + V_{shift}}{65.0}}}$$
$$k_{RIAI} = \frac{1}{0.0018 \cdot e^{\frac{V_m + V_{shift}}{-7.4}} + 2.0 \cdot e^{\frac{V_m + V_{shift}}{-100.0}}}$$
$$k_{AIRI} = \frac{1}{V_m + V_{shift} \quad V_m + V_{shift}}$$

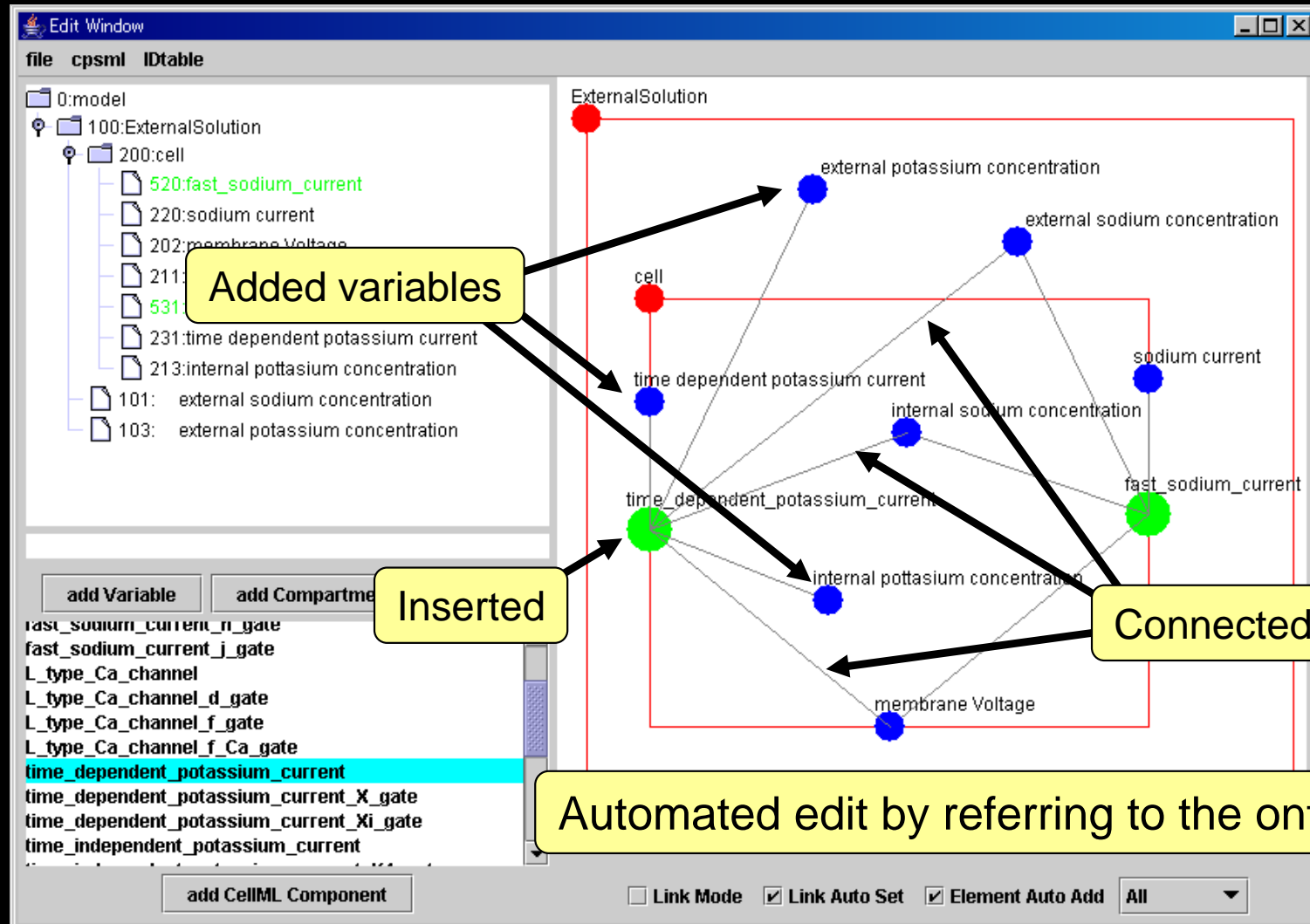
Annotation using ID of an ontology entry

Graphical display of equations with simple text input

Equation:  $k_{RIAI} = 1 / (0.0018 * \exp(((V_m + V_{shift}) / -7.4)) + (2.0 * \exp(((V_m + V_{shift}) / -100.0))))$

Description:

# Composition of Model



# Convertibility to CellML

- Export to CellML
  - Straightforward conversion
    - Usable as an authoring tool of CellML
- Import from CellML
  - Requires to assign ontology IDs to elements
    - A tool available to intelligently estimate ontology ID



# Experimental Protocol

- Simulation needs a model and an experimental protocol

Wet experiment

Computer simulation

Experimental protocol

Experimental protocol

apply

apply

Cell / tissue

Computational model

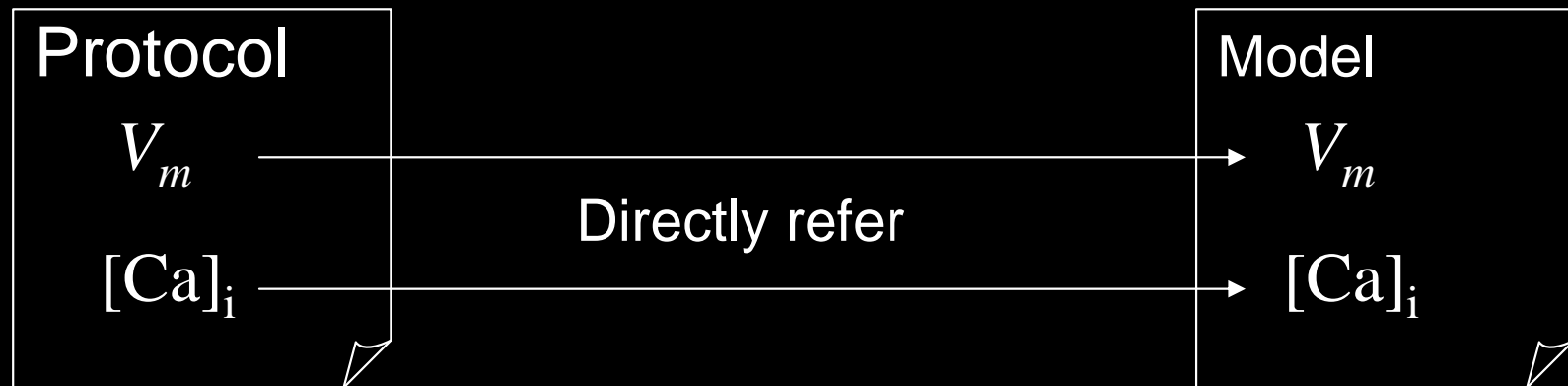


# PEPML

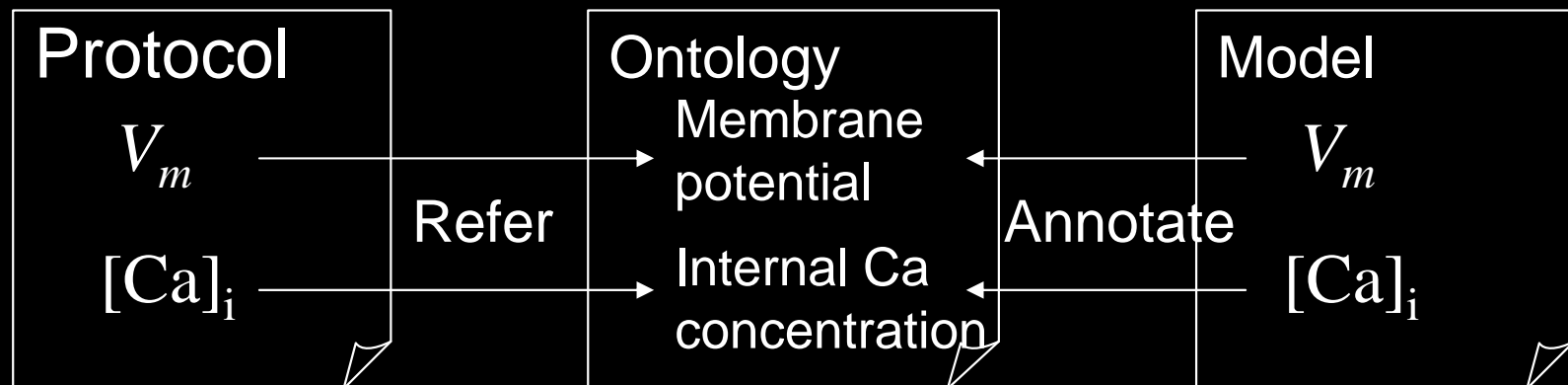
- Physiological Experimental Protocol ML
  - XML-based general format
  - Procedural representation  
vs. declarative representation
  - Model independent description using  
ontologies

# Reference of Model Variable

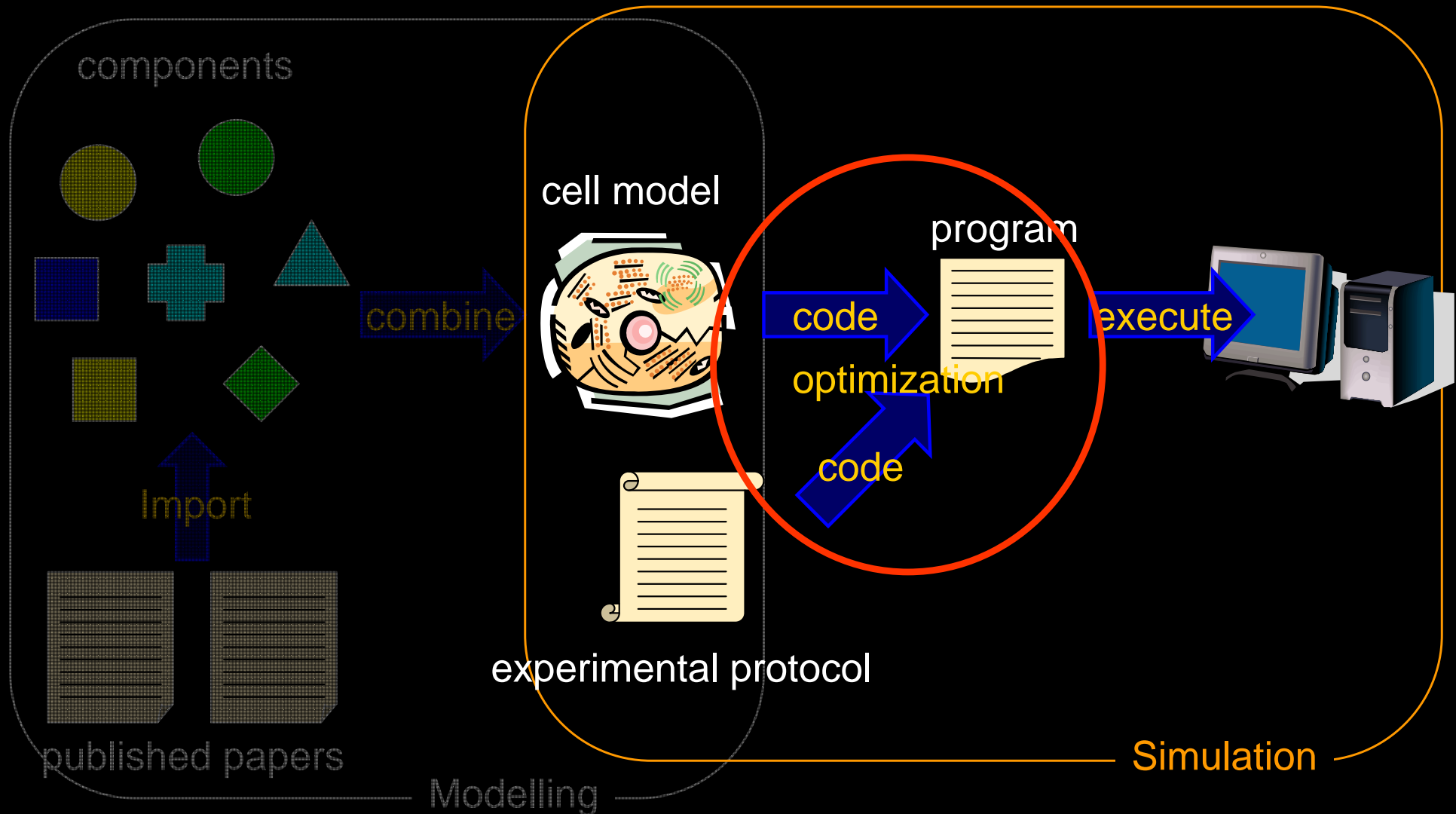
- Without ontology, model-specific



- With ontology, model-independent



# Difficulties in Simulation



# Boundary Conditions

- Models formulated as DAE:
  - ODE + simultaneous algebraic equations
- Consistent set of boundary conditions for correct simulation of DAE models
  - Which variables are given the values externally?

$$\begin{cases} p \cdot u - (q + a) \cdot v = c \\ (q + a) \cdot u^2 + p \cdot v^2 = d \end{cases}$$

# Difficulty

- Difficult to assign consistent boundary conditions to a model with hundreds of variables
- Wrong boundary conditions result in
  - Impossibility of calculation
  - Oblivious unintended calculation

# Setup of Boundary Conditions

- Assistance to assign a consistent set of boundary conditions based on graph theory
  - Automatic extraction of candidate variables to be bounded

cyclic AMP metabolism module [Saucerman 2003]

$$[G_{s\alpha}GTP] + [G_{s\alpha}GTP : AC] = [G_{s\alpha}GTP_{tot}]$$

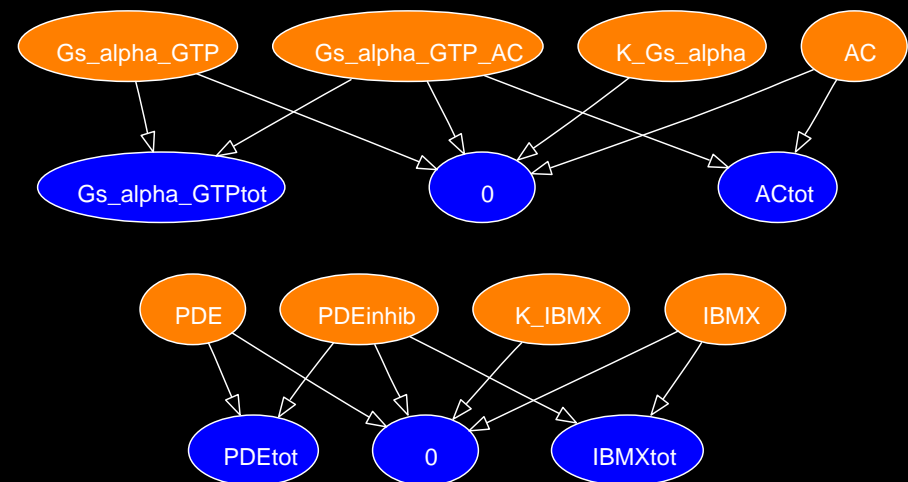
$$[G_{s\alpha}GTP : AC] + [AC] = [AC_{tot}]$$

$$[PDE_{inhib}] + [PDE] = [PDE_{tot}]$$

$$[PDE_{inhib}] + [IBMX] = [IBMX_{tot}]$$

$$[G_{s\alpha}GTP][AC] = K_{G_{s\alpha}}[G_{s\alpha}GTP : AC]$$

$$[PDE][IBMX] = K_{IBMX}[PDE_{inhib}]$$



# Automatic Optimization

- Optimization of simultaneous equations
  - Reduction of the degree

Original

degree: 3+3

$$[G_{s\alpha}GIP] + [G_{s\alpha}GIP : AC] = [G_{s\alpha}GIP_{tot}]$$

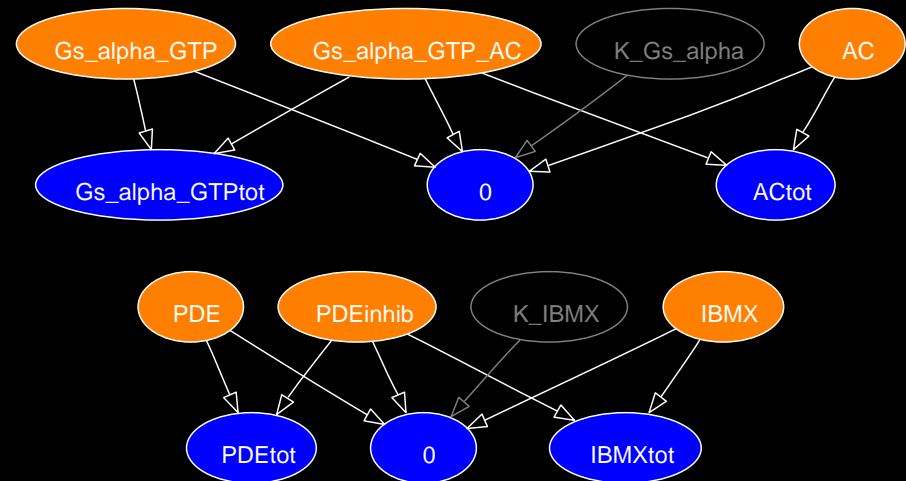
$$[G_{s\alpha}GIP : AC] + [AC] = [AC_{tot}]$$

$$[PDE_{inhib}] + [PDE] = [PDE_{tot}]$$

$$[PDE_{inhib}] + [IBMX] = [IBMX_{tot}]$$

$$[G_{s\alpha}GIP][AC] = K_{G_{s\alpha}}[G_{s\alpha}GIP : AC]$$

$$[PDE][IBMX] = K_{IBMX}[PDE_{inhib}]$$



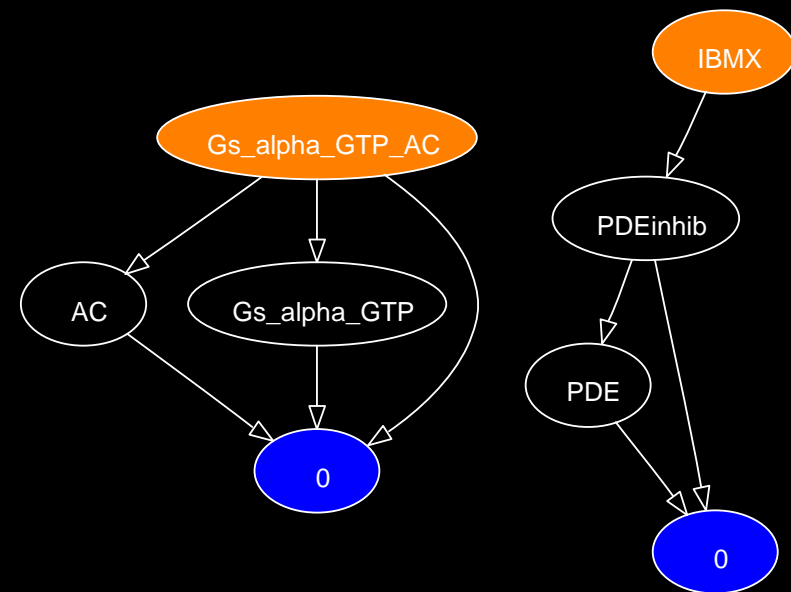


# Automatic Optimization

- Optimization of simultaneous equations
  - Reduction of the degree

After optimization      degree: 1+1

$$\begin{aligned}
 [G_{s\alpha GIP}] &= [G_{s\alpha GIP_{tot}}] - [G_{s\alpha GIP : AC}] \\
 [AC] &= [AC_{tot}] - [G_{s\alpha GIP : AC}] \\
 [G_{s\alpha GIP}][AC] - K_{G_{s\alpha}} [G_{s\alpha GIP : AC}] &= 0 \\
 [PDE_{inhib}] &= [IBMX_{tot}] - [IBMX] \\
 [PDE] &= [PED_{tot}] - [PDE_{inhib}] \\
 [PDE][IBMX] - K_{IBMX} [PDE_{inhib}] &= 0
 \end{aligned}$$



# Evaluation

- Beta signalling model [Saucerman 2003]
  - Unoptimized naïve math expressions
- Configuration of boundary conditions
  - #Candidates
    - Manual: 3060
    - With the proposed method: 516 (16.9%)
- Optimization of equations
  - Computation time
    - Without optimization: 31.5 [s]
    - With automatic optimization: 20.5 [s] (64.9%)

# Conclusion

- Easy modelling and simulation with information technology
  - Modelling with ontology
  - Protocol description format
  - Convenient simulation using graph theory
- Prototype software tools available on <http://www.biosim.med.kyoto-u.ac.jp/~simayosi/research/tools/>

*Thank you!*